

Review Article

A review of experimental studies for available experimental evidence on the use of prosthetic material in diaphragmatic hiatal hernia repair

ABSTRACT

Aim: The benefits of prosthetic material in hiatal hernia repair have been well documented. However, the associated risks are substantial and they are related to the technique, but also the choice of material. Experimental data are invaluable to understand and evaluate the interaction of different meshes with the host tissue. The purpose of this article is to summarize the available experimental evidence in the repair of hiatal hernias with the use of prosthetic materials in animal models.

Methods: A review of the literature from January 1990 to December 2014 was carried out for articles presenting experimental data on hiatal hernia repair.

Results: After discarding non relevant articles, 35 articles were identified. A variety of synthetic and absorbable materials were studied. Review of the available studies showed that there is great variability between synthetic materials regarding tissue integration, shrinkage and adhesion formation, however they have greater mechanical strength when compared to however biological/absorbable materials, which have a tendency for better integration in host tissue. Biological adhesives seem to be an effective alternative method of mesh fixation.

Conclusions: Experimental data are essential in order to fully appreciate the process of repair of a hiatal hernia with a prosthetic material. The articles reviewed provide insight into the properties of different prosthetic materials. However, there were large variations in their quality and the methods used. Data from animal studies are an excellent way of evaluating the multitude of materials that have recently become available. Good quality, comparative animal studies are essential in an effort to further improve outcomes for patients who undergo hiatal hernia repair.

Keywords: hiatal, hernia, diaphragmatic, mesh, animal, experimental, review

9 **1. INTRODUCTION**

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11
12 The introduction of laparoscopic techniques in hiatal hernia repair resulted in a significant increase
13 in the number of annually performed anti-reflux procedures in less than a decade [1]. There are now
14 randomized trials supporting the use of surgical management as a first-line treatment in selected patients
15 [2]. In some patient subgroups, however, such as the patients with a large paraesophageal hernia,
16 recurrence rates can reach 42% [3]. Recurrence usually occurs after disruption of the crural closure and
17 as the tissues being approximated are frequently attenuated and sutured under tension [4].

18 In an effort to overcome these limitations, selective mesh use has been reported since the 1970s.
19 In the first large series of patients published, Carlson et al were able to achieve excellent results with
20 polypropylene repair, without any clinical recurrences in long term follow up [5]. A number of clinical trials
21 have since established the efficacy of prosthetic mesh in preventing recurrence in the hiatus [6], however,
22 the emergence of relatively few, but in some cases devastating, complications such as mesh erosion,
23 highlight the need for further research [7].

24 As new materials are continuously being developed it is important for surgeons to make an
25 informed decision on which material to use. Animal studies are essential in evaluating the interaction
26 between the different prosthetic materials and the host tissue and their relative safety and efficacy in
27 hiatal hernia repair. We have performed a literature review in order to examine the contribution of the
28 available experimental evidence towards selecting the optimal prosthetic material and surgical technique
29 in mesh repair of hiatal diaphragmatic hernia.

30 **2. MATERIAL AND METHODS**

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34 We searched for articles on hiatal diaphragmatic hernia repair meeting the criteria outlined below
35 and analyzed them for specific outcomes using the PRISMA guidelines.

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37 **2.1 ELIGIBILITY CRITERIA**

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40 1) Type of study: Experimental animal (in vivo) study of repair of hiatal/paraesophageal or congenital
41 diaphragmatic hernia using prosthetic material (mesh). Models of congenital diaphragmatic hernia
42 were included in this review, because, although the mesh was not placed in the hiatus in these
43 models, they can be considered orthotopic models, usually involving creation of a hernia by excision
44 of part of the left hemidiaphragm, mimicking conditions like those found in a giant paraesophageal
45 hernia (large defect, attenuation of muscular tissue).

46 2) Language: English

47 3) Publication year: 1990-2014

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49 **2.2 LITERATURE SEARCH STRATEGY**

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51 Studies were identified by searching the PubMed/Medline and Scopus databases. The following
52 key words were used as search strings: hiatal, diaphragmatic, mesh, animal, experimental.

53 Potentially relevant articles were identified by the title and abstract and full papers were obtained
54 and assessed in detail by two of the authors (M.S. and P.T., both senior surgeons) prior to their inclusion
55 in the review. The reference list for each article was also screened to identify further relevant publications.

56

57 **2.3 Study selection**

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59 Eligibility assessment was performed independently by 2 reviewers. Disagreements between
60 reviewers were resolved by consensus.

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62 **2.4 Data extraction**

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64 Data collection and analysis were carried out independently by 2 researchers. Studies were
65 classified into two experimental model groups which investigated mesh repair of either hiatal or congenital
66 diaphragmatic hernia. Articles were reviewed for a number of variables examining their design (number
67 and type of animals, mesh implantation time, use of comparative/control group,

69 biomechanical/histopathological analysis) and the technique used (Mesh type and shape, fixation type,
70 surgical technique).

71 Study results were specifically assessed for findings relevant to controversial topics in hiatal
72 diaphragmatic hernia repair with prosthetic mesh (Table 1).

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Table 1: Controversial topics in hiatal hernia repair with prosthetic mesh

1. Mesh shape

2. Mesh type

a. Infection potential

b. Handling characteristics

c. Durability of repair

d. Adhesion potential, tissue incorporation, fibrosis/stenosis/shrinkage
potential

f. Migration/erosion potential

3. Fixation method

4. Sutured vs tension-free hiatoplasty

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75 **3. RESULTS**

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77 **3.1 Literature search**

78 Our search strategy initially returned 924 studies which we evaluated based on title and
79 abstract and we selected 21 articles based on our inclusion criteria. The full text of these articles was
80 downloaded and another 9 studies were obtained from their reference lists. After excluding 2 articles
81 studying hiatal hernia repair in the context of fetal tissue engineering, 28 articles were assessed in detail
82 (Figure 1).

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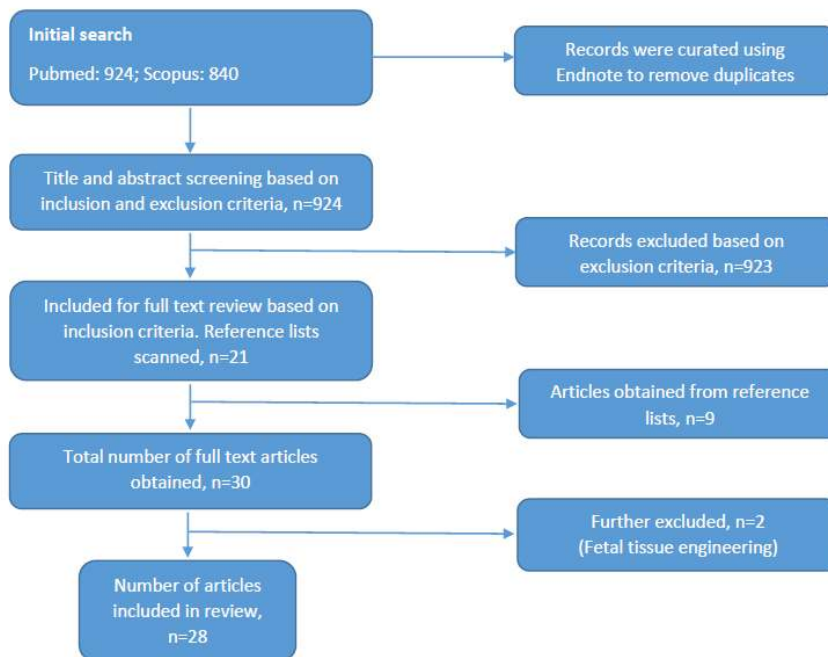
84 **3.2 Study design**

85 Large animals (swine, dogs) were used in most studies. The number of animals in each study was
86 small (6-36 animals). Implantation time ranged from 2 weeks to 12 months (Table 2). A majority of studies

87 included a comparison or control group and histopathological analysis, however only a few studies used
88 endoscopic or radiological assessment or biomechanical analysis.

89 **3.3 Mesh characteristics and surgical technique**

90 A variety of meshes were evaluated, including conventional (polypropylene,
91 polytetrafluoroethylene - PTFE) and newer (polypropylene/ polyglactin 910 - PP-PG, poly(lactic-co-
92 glycolic acid) - PLGA) synthetic materials, biologically derived materials such as bovine pericardium and
93 newer biologic meshes (Small intestinal submucosa - SIS, acellular dermal matrix - Alloderm). Most
94 authors used a rectangular piece of mesh, but circular and U-shaped meshes were also used. The
95 surgical technique used in most studies was mesh fixation in the hiatus using an open technique, with or
96 without excision of part of the left hemidiaphragm, while in two studies an endoscopic approach was
97 utilized: laparoscopic creation of a defect in the left hemidiaphragm and repair in one study and
98 thoracoscopic creation of a paraesophageal hernia and subsequent laparoscopic repair in another.
99 Finally, mesh fixation was achieved with sutures in most cases, while a few of the authors used biological
100 adhesives, such as fibrin glue and polyethylene glycol (Table 3).



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102 **Figure 1: Flow diagram of literature search**

103 **3.4 Results of individual studies**

104 **3.4.1 Mesh shape**

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106 Although circular, rectangular and U-shaped meshes were used, no study directly compared meshes of
107 different shapes. In a study of polypropylene meshes of a circular shape fixed by sutures in a rabbit
108 model, the meshes had usually moved from their implantation bed and had eroded into the esophagus
109 [16]. However, in another study a circular polypropylene mesh was fixed in place using fibrin glue in a
110 swine experimental model and in this case the authors reached conflicting results as they found the
111 meshes stayed in position and their inner edge had retracted evenly from the esophagus [14].

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113 **3.4.2 Mesh type**

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116 *3.4.2.1 Infection potential*

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118 No study on mesh use in contaminated fields has been carried out.

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120 *3.4.2.2 Handling characteristics*

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122 The handling characteristics of each mesh i.e. the ease of its use in laparoscopic surgery was not
123 addressed in any study.

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125 *3.4.2.3 Durability of repair*

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127 Most of the studies discussed showed that the mesh repair remained successful during the observation
128 period of up to 12 months. SIS was shown to have equivalent strength to PTFE when applied on the
129 diaphragm [27, 32], although it was not as strong as polypropylene meshes [25, 26]. In another study
130 comparing two forms of SIS mesh in a dog model, the first comprised of 4-ply and the other from 8-ply,
131 the thicker version was shown to be stronger, while both showed more strength than native diaphragmatic
132 tissue [28]. Fascia lata was also shown to be equivalent to PTFE in mechanical strength [29].

133 3.4.2.4 Adhesion potential, tissue incorporation, fibrosis/stenosis/shrinkage potential

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135 Polypropylene mesh consistently caused formation of strong adhesions [25, 26], which were less
136 pronounced with low-weight polypropylene [9]. Dualmesh showed less extensive adhesions than
137 polypropylene [17], while Surgisis showed less adhesions than PTFE in two studies [11, 32], but dense
138 adhesions comparable to polypropylene in another [25].

139 Mesh shrinkage was shown to be around 50-70% of original size for polypropylene [9, 14, 16], while the
140 percentage of shrinkage was more for the low-weight mesh [9]. When PTFE, polyester and polypropylene
141 were compared, PTFE showed considerably more shrinkage that reached 34.9% of its original size [8].

142 Bohm et al compared two composite synthetic polypropylene meshes (Ultrapro, Proceed) to
143 Surgisis in a rabbit model [25, 26]. Inflammatory reaction at the border of the mesh was more pronounced
144 with Proceed, followed by Ultrapro and Surgisis. On the other hand Surgisis and Ultrapro showed better
145 tissue regeneration compared to Proceed. Collagen maturation was slower for Surgisis compared to the
146 synthetic meshes. A composite polypropylene mesh was compared to a conventional polypropylene
147 mesh and the composite mesh showed better integration and reduced inflammatory response, which
148 could be associated with a lower risk of erosion and postsurgical dysphagia [16]. Histological examination
149 and cross-polarization microscopy showed differences in cell proliferation rate, apoptosis and collagen
150 I/III ratio, which were statistically significant and show better tissue integration for the composite mesh
151 [15, 16] Another study showed excellent integration, for a titanium-polypropylene mesh [13].

152 Polytetrafluoroethylene (ePTFE/ Dualmesh) was evaluated and caused the formation of minimal
153 adhesions except in segments of the mesh where folding exposed its superior surface. There were no
154 erosions or migration noted. Microscopic evaluation showed only an unstable capsule encompassing the
155 mesh underlining the importance of a stable fixation [17, 24, 33].

156 Biologically-derived materials were evaluated in several studies. The authors reported complete
157 mesh replacement by fibrovascular scar tissue with SIS mesh, with significant muscular regeneration,

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Table 2: Design of experimental studies in hiatal diaphragmatic hernia repair

| | Author | Pub year | Animal type | N | Implantation time | Comparative/control group | Biomechanical analysis | Histopathological analysis | Endoscopic/radiological assessment |
|--|-------------------|----------|-------------|----|-----------------------|---------------------------|------------------------|----------------------------|------------------------------------|
| <i>Hiatal hernia repair models</i> | | | | | | | | | |
| 1 | Muller-Stich [8] | 2014 | Swine | 24 | 8 weeks | ✓ | | ✓ | |
| 2 | Senft [9] | 2014 | Swine | 24 | 8 weeks | ✓ | | | |
| 3 | Krpata [10] | 2012 | Swine | 20 | 30 days | | | | |
| 4 | Vereczkei [11] | 2012 | Dogs | 3 | 1/3/6 months | ✓ | | ✓ | |
| 5 | Jenkins [12] | 2011 | Swine | 32 | 2 weeks | | | | |
| 6 | Fortelny [13] | 2010 | Swine | 7 | 4 weeks | | | ✓ | |
| 7 | Muller-Stich [14] | 2008 | Swine | 9 | 6 weeks | | | ✓ | |
| 8 | Otto [15] | 2008 | Rabbits | 20 | 3 months | ✓ | | ✓ | |
| 9 | Jansen [16] | 2007 | Rabbits | 20 | 3 months | ✓ | ✓ | | ✓ |
| 10 | Smith [17] | 2007 | Swine | 18 | 3/28 weeks | ✓ | | ✓ | |
| 11 | Desai [18] | 2006 | Dogs | 6 | 12 months | | | ✓ | ✓ |
| <i>Congenital diaphragmatic hernia repair models</i> | | | | | | | | | |
| 12 | Brouwer [19] | 2013 | Lambs | 7 | 6 months | ✓ | | ✓ | |
| 13 | Zhao [20] | 2013 | Rats | 52 | 1, 2, 4, and 6 months | ✓ | | ✓ | |
| 14 | Brouwer [21] | 2013 | Rats | 36 | 12 weeks | ✓ | | ✓ | |
| 15 | Brouwer [22] | 2013 | Rats | 36 | 2/12 weeks | ✓ | | ✓ | |
| 16 | Brouwer [23] | 2013 | Rats | 25 | 2/4/8/12/24 weeks | ✓ | | ✓ | |
| 17 | Gonzalez [24] | 2011 | Swine | 20 | 6 months | ✓ | | ✓ | |
| 18 | Bohm [25] | 2010 | Rabbits | 33 | 4 months | ✓ | | ✓ | |
| 19 | Bohm [26] | 2010 | Rabbits | 33 | 4 months | ✓ | ✓ | | |
| 20 | Urita [27] | 2008 | Rats | 24 | 1-3 months | | | | |
| 21 | Sandovalb [28] | 2006 | Dogs | 11 | 6 months | ✓ | ✓ | ✓ | |
| 22 | Suzuki [29] | 2002 | Dogs | 24 | 15/30 days | | | | |
| 23 | Upadhyaya [30] | 2001 | rat | 8 | 3 weeks | ✓ | ✓ | ✓ | |
| 24 | Steinau [31] | 2000 | pigs | 24 | 3/6 months | ✓ | ✓ | ✓ | |
| 25 | Lantis II [32] | 2000 | Rabbits | 32 | 6/12 weeks | ✓ | ✓ | ✓ | |
| 26 | Kimber [33] | 2000 | Lambs | 12 | 1,3,6 months | ✓ | ✓ | | |
| 27 | Dalla Vecchia[34] | 1999 | Rats | 87 | 2 weeks - 4 months | ✓ | | ✓ | |
| 28 | Lally [35] | 1993 | Rats | 37 | 400 gr | ✓ | | ✓ | |

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161 without any erosion in surrounding hollow viscera [18]. The 8-ply SIS mesh shows a slower rate of
162 degradation compared to the 4-ply, which can in turn lead to better integration into host tissue [28]. SIS
163 shows equivalent capillary ingrowth to Alloderm (acellular human cadaveric dermis), but a higher level of
164 thinning [34]. When compared to PTFE, SIS shows better integration [11], more collagen deposition and
165 skeletal muscle regeneration and neovascularization [24]. Finally, fascia lata showed superior integration
166 and capillary ingrowth to ePTFE [29] and, in a separate study, excellent tissue integration and
167 neovascularization, along with a mild to moderate inflammatory reaction [11].

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169 *3.4.2.5 Migration/erosion potential*

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171 In a study of polypropylene meshes of a circular shape fixed by sutures in a rabbit model, the meshes
172 had usually moved from their implantation bed and had eroded into the esophagus [16]. However, in
173 another study a circular polypropylene mesh was fixed in place using fibrin glue in a swine experimental
174 model and in this case the authors reached conflicting results as they found the meshes stayed in
175 position and their inner edge had retracted evenly from the esophagus [14].

176 The level of migration and the extent of foreign body reaction were higher when a conventional
177 polypropylene mesh was used compared to a composite one [15, 16]. The part of the mesh close to the
178 diaphragm showed less mechanical stability compared to the one close to the esophagus. In a
179 comparative study of PTFE and SIS in a pig model of congenital diaphragmatic hernia repair, the authors
180 were able to demonstrate PTFE has a poorer integration into host tissue compared to SIS and tends to
181 migrate and fold [24].

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183 **3.4.3 Fixation method (sutures/tacks/glue)**

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185 Biologically compatible adhesives like fibrin glue and polyethylene glycol were used with no evidence of
186 migration, no evidence of any adverse effect to the incorporation of the mesh and equivalent strength to
187 suture fixation. Krpata et al used an acellular porcine dermal matrix and compared fibrin sealant to
188 fixation with sutures [10]. Meshes fixed with fibrin glue showed no folding, while there was minimal folding

189 in the control group. Esophagograms did not exhibit any signs of strictures. The authors used a “peel” test
190 to compare the force needed to separate the mesh from the crura and found no difference between the
191 two techniques, whilst the introduction of glue between the crura and the mesh did not result in a
192 significantly different cellular response. Use of fibrin sealant resulted in a significant reduction in operative
193 time. Jenkins et al compared two biological adhesives and found both equally effective in mesh fixation
194 [12]. In conclusion data from 6 experimental studies show that both adhesives seem very promising as an
195 alternative, safe, faster fixation method in hiatal hernia repair.

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197 **3.4.4 Sutured or tension free hiatoplasty**

198 In reviewing the available published studies we did not find any study comparing sutured to tension-free
199 hiatoplasty.

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201 **4. DISCUSSION**

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205 There are a number of controversial points regarding the best surgical technique in hiatal and
206 paraesophageal hernia surgery [36], the most controversial of which concerns the placement of mesh in
207 the oesophageal hiatus [37-39]. There are reports of a significant reduction in recurrence rates when
208 mesh is used in the surgical repair of hiatal hernia [40, 41]. On the other hand, the surgical community is
209 now conscious that there are important drawbacks in the form of mesh-related complications, reports of
210 which were scarce for two decades and have now begun to appear in the literature [7, 42, 43].
211 **Polypropylene mesh in the hiatus can cause devastating complications including dense fibrosis,**
212 **oesophageal stenosis and intraluminal mesh erosion, the management of which may necessitate a**
213 **reoperation ranging from mesh removal to oesophagectomy [7].** A mesh placed in the diaphragm is
214 subjected to the constant movements of breathing, which are likely to affect its incorporation to the host
215 tissue. Therefore, although there are multiple articles available studying mesh use in animal models for a
216 variety of indications, it is important to evaluate results from animal models of **hiatal diaphragmatic** hernia
217 repair.

218 Our literature review showed that there were large variations in the quality of experimental studies,
219 only a few of which incorporated histopathological, biomechanical, endoscopic and radiological

219 assessment. The number of animals was small and the implantation time was limited. The surgical
 220 technique used in most cases is a disadvantage, since
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Table 3: Mesh characteristics and surgical technique

| Mesh type | Mesh shape | Surgical technique | Fixation method | |
|--|---|--------------------|--|--|
| <i>Hiatal hernia repair models</i> | | | | |
| 1 [8] | PP/ PET/ PTFE | Circular | Open hiatoplasty and placement of patch in the oesophageal hiatus | Fibrin glue |
| 2 [9] | heavyweight small-porous/heavyweight large-porous/lightweight large-porous PP | Circular | Open hiatoplasty and placement of patch in the oesophageal hiatus | Fibrin glue |
| 3 [10] | acellular porcine dermal matrix | U shaped | Laparoscopic hiatal hernia repair | Sutures/Fibrin sealant |
| 4 [11] | Pericardial and fascia lata patches | Rectangle | 3x3 cm patches fixed on muscular part of diaphragm | Polypropylene 3/0 |
| 5 [12] | SIS | U shaped | Laparoscopic placement of patch in oesophageal hiatus | Fibrin glue/ polyethylene glycol |
| 6 [13] | Titanium polypropylene mesh | Keyhole | Open placement of the patch without prior hiatoplasty | Fibrin glue |
| 7 [14] | Heavy-weight polypropylene | Circular | Open hiatoplasty and placement of patch in the oesophageal hiatus | Fibrin glue |
| 8 [15] | PP/ PP–polyglactone 25 composite | Circular | Open hiatoplasty and placement of patch in the oesophageal hiatus | Polypropylene 6/0 |
| 9 [16] | PP/ PP–polyglactone 25 composite | Circular | Open hiatoplasty and placement of patch in the oesophageal hiatus | Polypropylene 6/0 |
| 10 [17] | DualMesh | U shaped | Open transabdominal excision of left hemidiaphragm and open placement of patch in the oesophageal hiatus without prior hiatoplasty | Interrupted ePTFE |
| 11 [18] | SIS | U shaped | Thoracoscopic creation of diaphragmatic hernia and subsequent laparoscopic repair, with hiatoplasty and placement of patch | Interrupted 2/0 polyester |
| <i>Congenital diaphragmatic hernia repair models</i> | | | | |
| 12 [19] | Collagen-Vicryl | Rectangle | Posterolateral 3x1.5 cm diaphragmatic defect | Running 4/0 prolene |
| 13 [20] | poly(ε-caprolactone) and collagen type I | Rectangle | Excision of 70% of the left hemi-diaphragm (approximately 2-3 cm ²) | Interrupted 6/0 Prolene |
| 14 [21] | Dual layered collagenous scaffolds | Rectangle | 12 mm diameter right diaphragm defect | Interrupted 6/0 Prolene |
| 15 [22] | Cross-linked collagenous scaffolds | Rectangle | 12 mm diameter right diaphragm defect | Interrupted 6/0 Prolene/ interrupted 5/0 Vicryl |
| 16 [23] | Cross-linked collagenous scaffolds | Rectangle | Excision of 1/3 of the right hemidiaphragm | Interrupted 6/0 Prolene |
| 17 [24] | SIS, ePTFE | Rectangle | Excision of the left hemidiaphragm | Running 3/0 prolene |
| 18 [25] | SIS, PP plus Polyglactone-25, and PP plus polydioxanone and cellulose plus Tachosil | Rectangle | A defect of 1cm in diameter was made into the lateral left diaphragm at the interface of tendon and muscle | Running 5/0 Prolene |
| 19 [26] | SIS, PP plus Polyglactone-25, and PP plus polydioxanone and cellulose plus Tachosil | Rectangle | A defect of 1cm in diameter was made into the lateral left diaphragm at the interface of tendon and muscle | Running 5/0 Prolene |
| 20 [27] | PLGA - collagen mesh | Rectangle | Open transabdominal left hemidiaphragm excision and repair | N/A |
| 21 [28] | SIS | Rectangle | Open transabdominal left central hemidiaphragm excision and repair | N/A |
| 22 [29] | Autologous fascia lata/ ePTFE | Rectangle | Left thoracotomy, left hemidiaphragm excision and repair | N/A |
| 23 [30] | Integra | Rectangle | Open excision of left hemidiaphragm and patch repair | Interrupted 6/0 Vicryl |
| 24 [31] | lyophilized dura/ transverse abdominal bovine | Rectangle | Open excision of left hemidiaphragm and patch repair | Polypropylene 3-0 |

| | | | | |
|---------|--|-----------|---|-----------------------|
| | pericardial serosa | | | |
| 25 [32] | SIS/ PTFE | Rectangle | Open transabdominal left hemidiaphragm excision and repair | N/A |
| 26 [33] | PTFE/ fluoropolymer-coated PET | Rectangle | Laparoscopic creation of 2x2 cm defect in left hemidiaphragm and repair | 3-0 braided polyester |
| 27 [34] | SIS/AlloDerm | Rectangle | Open transabdominal left central hemidiaphragm excision and repair | N/A |
| 28 [35] | ePTFE/oxidized cellulose/polyglactin 910 | Rectangle | Excision of the left hemidiaphragm followed by repair with a patch | Running 4-0 silk. |

SIS: small intestinal submucosa; PTFE: polytetrafluoroethylene; PP: polypropylene; PLGA: poly(lactic-co-glycolic acid); PET: polyester

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223 neither the creation of a hiatal hernia nor minimally invasive techniques were used, although similar
 224 experimental models have been described as in the article by Desai et al, where a study incorporating the
 225 creation of a diaphragmatic hernia and its subsequent repair using laparoscopy is presented, in a model
 226 closely resembling the current clinical practice and enabling the surgeon to appreciate the handling
 227 characteristics of each mesh [18]. Finally, due to the heterogeneity of the studies quantitative analysis of
 228 the results was not possible.

229 We evaluated studies regarding specific topics and a number of these were not addressed at all
 230 (infection potential, handling characteristics, sutured/ tension free hiatoplasty), while there was limited
 231 data on the impact of mesh shape and the migration/erosion potential and durability of each mesh.

232 A test of the durability of the hiatoplasty should ideally compare biological/bioabsorbable
 233 prostheses to materials like polypropylene or PTFE, the efficacy of which has been demonstrated in
 234 randomized trials [40, 41]. Biological meshes made from small intestinal submucosa have been shown to
 235 reduce recurrence rates in a randomized trial with short-term follow-up [44] and can also be used as a
 236 control to evaluate newer biological materials. The ability of the mesh to prevent recurrence can be
 237 investigated at autopsy or radiologically. However, new recurrences have been known to occur for a long
 238 time after surgery. Indeed, long term observation of the patients in the previously mentioned trial showed
 239 no benefit in recurrence rates with SIS mesh [45]. The practical limitations of observation time in animal
 240 studies lead authors to perform biomechanical evaluation of mesh materials to evaluate the durability of
 241 the repair. Results confirm the better results obtained clinically with polypropylene compared to biologics,
 242 but are surprising since PTFE was weaker than expected [40].

243 Most of the authors focused on the potential of adhesion formation, biocompatibility and tissue
 244 integration of each mesh and adequate experimental data on several materials is available. The safety
 245 profile of each material i.e. its potential to adhere to and erode into viscera, to cause extended fibrosis

246 resulting in oesophageal stenosis, or to migrate from its position is the most pressing issue, since it is the
247 reason mesh-augmented hiatoplasty is not widely used in clinical practice. Polypropylene meshes
248 showed good integration, but also caused significant adhesions. Experimental studies will be very useful

Table 4: Summary of results

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1. Mesh shape : no differences
 2. Mesh type
 - a. Infection potential : no differences
 - b. Handling characteristics : no differences
 - c. Durability of repair : Polypropylene stronger than PTFE, biologics
 - d. Adhesion potential, tissue incorporation, fibrosis/stenosis/*shrinkage* potential:
 - More adhesions with synthetic meshes, especially polypropylene.
Significant amount of shrinkage for PTFE, but also polypropylene.
 - Better integration for composite compared to conventional polypropylene, unstable integration for PTFE.
 - Better tissue integration and regeneration for SIS compared to synthetic materials.
 - f. Migration/erosion potential : PTFE has a poorer integration compared to SIS, while composite is better than conventional polypropylene,
 3. Fixation method: Biologically compatible adhesives comparable to suture fixation

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250 for the comparison of the new generation lightweight meshes, so as to evaluate their advantages
251 compared with standard polypropylene meshes. PTFE resulted in less adhesions, but poor integration
252 with the host tissue. SIS mesh showed an excellent safety profile in experimental studies. These results
253 are in accordance with those obtained from clinical trials including a prospective randomized trial [44] but
254 a marked fibrous response was observed in a previous comparative experimental study, published in
255 abstract form, where significant esophageal stenosis was shown [46]. This finding is significant since
256 esophageal stenosis have been reported in clinical series of patients operated on with SIS mesh [7].

257 The method used to fix the prosthesis to the crura presents a problem since laparoscopic suturing
258 is challenging and time consuming (and potentially risky for the inexperienced) and use of tacks, although
259 fast and effective, places large vessels and the heart at risk of serious injury with potentially catastrophic
260 results [47]. The stability of the mesh depends on both the fixation method but also the material itself and
261 the strength of its incorporation. T-peel testing is an elegant method of quantifying the strength of mesh
262 incorporation [10]. Directly observing the tendency of the mesh to migrate and cause adhesions is
263 tempting, however results must be interpreted with caution; failure of known complications to emerge in
264 these studies could be caused by the relatively short observation time (erosions occur up to nine years
265 after surgery) [7], but could also be interpreted to a lesser extent as proof of the importance of surgical
266 technique (i.e. to strengthen the argument that the reported complications are not inherent in the mesh
267 type but rather are a result of inadequate surgical technique). Indeed, there was a striking difference in
268 mesh migration of polypropylene mesh in the article by Fortelny et al compared to the study of Jansen et
269 al [13, 16]; the difference in the ratio of thickness between the mesh and the tissues of the two different
270 animal models was offered as an explanation.

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272 **5. CONCLUSION**
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274 The introduction of the new collagen-based biomaterials and the preliminary encouraging results
275 from their use raised great expectations for improved outcomes. The biomaterials from porcine small
276 intestinal submucosa and porcine or human acellular dermis are already widely used in clinical practice
277 (they were being used in 1/3 of all mesh-augmented hiatal diaphragmatic hernia repairs a few years ago
278 [48]) and experimental data are invaluable to further our understanding of their incorporation in host
279 tissue. Fascia lata has been used as a prosthetic material in the hiatus during the 1970s with mixed
280 results, showing efficacy but also some complications [49]. It is, however, in our opinion a very interesting
281 material because it is the only easily obtainable strong autologous patch and has been shown to possess
282 strength equal to PTFE and better incorporation on the diaphragm [28]. Although, the reviewed articles
283 study most of the types of meshes currently in clinical use, new biological and bioabsorbable materials
284 are being introduced in clinical practice without any available published experimental data [49, 50].

285 There is an ever growing need for experimental studies, which should also be well-designed in
286 order to also tackle ethical concerns with regards to animal sacrifice. Studies on mesh-augmented
287 hiatoplasty should include a laparoscopic animal model, biomechanical evaluation and histopathological
288 evaluation of no less than two different biomaterials at the very minimum. In the absence of good quality
289 clinical trials, which are invariably difficult to put together due to the relatively small number of patients,
290 good quality, comparative animal studies are essential in order to identify the mesh with the best
291 safety/efficacy profile, determine the optimal shape and fixation method and enable surgeons to make an
292 inform decision on the merits of using mesh in hiatal hernia repair.

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